

Seizure Classification From EEG Signals Using Transfer Learning, Semi-Supervised Learning and TSK Fuzzy System

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Abstract—Recognition of epileptic seizures from offline EEG signals is very important in clinical diagnosis of epilepsy. Compared with manual labeling of EEG signals by doctors, machine learning approaches can be faster and more consistent. However, the classification accuracy is usually not satisfactory for two main reasons: the distributions of the data used for training and testing may be different, and the amount of training data may not be enough. In addition, most machine learning approaches generate black-box models that are difficult to interpret. In this paper, we integrate transductive transfer learning, semi-supervised learning and TSK fuzzy system to tackle these three problems. More specifically, we use transfer learning to reduce the discrepancy in data distribution between the training and testing data, employ semi-supervised learning to use the unlabeled testing data to remedy the shortage of training data, and adopt TSK fuzzy system to increase model interpretability. Two learning algorithms are proposed to train the system. Our experimental results show that the proposed approaches can achieve better performance than many state-of-the-art seizure classification algorithms.

Index Terms—EEG recognition, seizure classification, transductive transfer learning, semi-supervised learning, TSK fuzzy system.

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I. INTRODUCTION

EPILEPSY is a common neurological disorder in which clusters of nerve cells in the brain function abnormally and cause seizures. Electroencephalogram (EEG) signals are commonly used to determine the presence and the type of epilepsy [1], [2]. As it is very time-consuming for doctors to label the EEG signals manually, researchers have studied machine learning approaches to automatically detect seizures from EEG signals [3]–[11]. Many different methods, including decision tree [9], naïve Bayes [7], [9], support vector machine [6], [11], nearest-mean [7] and linear discriminant analysis [5], [8], [10], have been applied.

Compared with manual labeling, detection by machine learning methods is faster and more consistent. However, the detection accuracy could be an issue. Yang *et al.* [12] pointed out that the main reason for low detection accuracy is that most machine learning methods are developed based on the assumption that the distributions of the training and testing data are identical or similar, which may not be true in practice. For example, a classifier may be trained using data from a repository of existing subjects and then applied to a new subject. To cope with this issue, transfer learning (TL) [13]–[18], [40], [42], particularly, large margin projection (LMPROJ) [18], has been used to reduce the data distribution mismatch between the training and testing data. The results demonstrate that TL is very suitable for this problem.

This paper also utilizes LMPROJ TL to improve seizure classification performance. It further considers two more problems: 1) how to increase model interpretability which is very important in medical diagnostics, and 2) how to make use of the information contained in the unlabeled testing data to improve classification performance. To deal with the first problem, we adopt the Takagi-Sugeno-Kang (TSK) fuzzy system [19]–[22], which is intrinsically interpretable, as our base classifier. For the second problem, in addition to LMPROJ, we use a semi-supervised learning (SSL) approach to take advantage of the unlabeled testing data. We also propose two learning algorithms for this TL-SSL-TSK based model and demonstrate its outstanding performance.

The rest of this paper is organized as follows. Section II briefly reviews the typical feature extraction and machine learning methods that are used for epileptic EEG recognition. Section III introduces the TSK fuzzy system model and the learning algorithm. Section IV introduces the details of the proposed TL-SSL-TSK model and the two learning algorithms developed for the model. Section V compares the performance of the proposed algorithms with that of existing methods on six real EEG datasets. Section VI concludes the findings of the study.

II. RELATED WORK

This section provides a brief review of typical methods used for EEG feature extraction and classification.

A. Feature Extraction Methods

Signal processing methods are used to extract features from the original raw EEG signals that are more concise and powerful to improve the classification performance [12], [23]–[29], [43] and to reduce the computational cost [4], [7], [8]–[10], [12], [23]–[29]. In general, there are three types of features: 1) time-domain features [23], [25], e.g. principal component features of the raw EEG signals, 2) frequency-domain features [3], [24], e.g. Fourier transform features, and 3) time-frequency features [3], [25]–[27], e.g. wavelets. All these three types of features will be considered in this paper.

B. Machine Learning Approaches

Machine learning methods can potentially detect seizures from EEG signals more quickly and consistently than manual labeling by doctors. If well trained, the methods can also achieve very high accuracy. Many classical machine learning methods have been studied for this purpose, such as decision tree [9], naïve Bayes [7], [9], support vector machine [6], [11], nearest-mean [7] and linear discriminant analysis [5], [8], [10].

Traditional machine learning methods usually assume that the distribution of the training and testing data are consistent, but they are indeed different in many real-world situations. As a result, the testing performance could be much worse than the training performance. TL [13] is a well-known approach for handling data distribution discrepancy. For example, Yang *et al.* [12] have used LMPROJ [18], a transductive TL algorithm, for seizure detection using EEG signals and achieved outstanding performance.

Another problem with many existing machine learning approaches is that black-box models can only be obtained, which lack the interpretability that is very important in medical diagnostics. In this paper, intrinsically interpretable TSK fuzzy system is used as our base model.

III. TSK FUZZY SYSTEM MODEL

The Mamdani model [20] and the TSK model [21], [22], [38] are two popular fuzzy system models. The latter is adopted in this study due to its simplicity and flexibility. This section introduces the TSK fuzzy system model and the corresponding training algorithm. The integration of the model with TL and SSL for achieving better classification performance will be discussed in the next section.

A. Concept and Principle

TSK fuzzy system is a rule based system. A typical rule can be described as TSK fuzzy rule R^k :

$$\text{IF } x_1 \text{ is } A_1^k \wedge x_2 \text{ is } A_2^k \wedge \cdots \wedge x_d \text{ is } A_d^k \quad (1)$$

THEN $f^k(\mathbf{x}) = p_0^k + p_1^k x_1 + \cdots + p_d^k x_d$ for $k = 1, \dots, K$ where K is the number of fuzzy rules, d is the number of inputs, A_i^k is a fuzzy set in the i th input domain for the k th rule, and \wedge is a fuzzy conjunction operator. Each rule is premised on the input vector $\mathbf{x} = [x_1, x_2, \dots, x_d]^T$ which is mapped to a singleton $f^k(\mathbf{x})$, a linear function of the input. The output of the TSK fuzzy system is computed as

$$y^0 = \sum_{k=1}^K \frac{\mu^k(\mathbf{x}) f^k(\mathbf{x})}{\sum_{k'=1}^K \mu^{k'}(\mathbf{x})} = \sum_{k=1}^K \tilde{\mu}^k(\mathbf{x}) f^k(\mathbf{x}), \quad (2.a)$$

where

$$\mu^k(\mathbf{x}) = \prod_{i=1}^d \mu_{A_i^k}(x_i) \quad (2.b)$$

and

$$\tilde{\mu}^k(\mathbf{x}) = \mu^k(\mathbf{x}) / \sum_{k'=1}^K \mu^{k'}(\mathbf{x}) \quad (2.c)$$

in which $\mu_{A_i^k}(x_i)$ is the membership grade of x_i on A_i^k [17], [22].

Gaussian membership function is used in this paper:

$$\mu_{A_i^k}(x_i) = \exp\left(\frac{-(x_i - c_i^k)^2}{2\delta_i^k}\right), \quad (2.d)$$

where

$$c_i^k = \sum_{j=1}^N u_{jk} x_{ji} / \sum_{j=1}^N u_{jk}, \quad (2.e)$$

$$\delta_i^k = h \cdot \sum_{j=1}^N u_{jk} (x_{ji} - c_i^k)^2 / \sum_{j=1}^N u_{jk}, \quad (2.f)$$

in which N is the total number of dataset. u_{jk} denotes the fuzzy membership and can be obtained by Fuzzy C-means (FCM) clustering or the likes [30], [39]. h is a scaling parameter which can be set manually, or optimized by some learning strategies such as cross-validation.

Denote

$$\mathbf{x}_e = (1, \mathbf{x}^T)^T, \quad (3.a)$$

$$\tilde{\mathbf{x}}^k = \tilde{\mu}^k(\mathbf{x}) \mathbf{x}_e, \quad (3.b)$$

$$\mathbf{x}_g = ((\tilde{\mathbf{x}}^1)^T, (\tilde{\mathbf{x}}^2)^T, \dots, (\tilde{\mathbf{x}}^K)^T)^T, \quad (3.c)$$

$$\mathbf{p}^k = (p_0^k, p_1^k, \dots, p_d^k)^T \quad (3.d)$$

$$\mathbf{p}_g = ((\mathbf{p}^1)^T, (\mathbf{p}^2)^T, \dots, (\mathbf{p}^K)^T)^T, \quad (3.e)$$

(2.a) can then be expressed as [17], [22]:

$$y^0 = \mathbf{p}_g^T \mathbf{x}_g. \quad (3.f)$$

B. Learning Algorithm for TSK Fuzzy Model

Given a training dataset of EEG signals (source domain) $D_S = \{\mathbf{x}_i, \mathbf{y}_i | \mathbf{x}_i \in R^d, \mathbf{y}_i \in R^C, i = 1, \dots, N_S\}$, the least squares method can be used to optimize the consequent parameters \mathbf{p}_g . The objective function is:

$$\min_{\mathbf{p}_g} J_{TSK}(\mathbf{p}_g) = \frac{1}{2} \sum_{j=1}^C \sum_{i=1}^{N_S} \left\| \mathbf{p}_{g,j}^T \mathbf{x}_{gi} - y_{ij} \right\|^2 + \frac{\lambda_1}{2} \sum_{j=1}^C \mathbf{p}_{g,j}^T \mathbf{p}_{g,j}, \quad (4)$$

where C is the number of classes, $\mathbf{p}_{g,j}$ is the consequent parameter vector of the j th class, \mathbf{x}_i is the d -dimension input vector of the i th sample, \mathbf{y}_i is the C -dimension label vector of the i th sample ($y_{ij} = 1$ when the i th sample belongs to the j th class; otherwise, $y_{ij} = 0$), and $\lambda_1 > 0$ is a regularization parameter, which controls the tradeoff between the complexity of the classifier and the tolerance of error. λ_1 can be set manually or determined by cross-validation [31].

The minimum of $J_{TSK}(\mathbf{p}_g)$ is obtained when the derivative of J_{TSK} w.r.t. each $\mathbf{p}_{g,j}$ is zero. The solution is:

$$\mathbf{p}_{g,j} = (\lambda_1 \mathbf{I}_{((d+1)*K) \times ((d+1)*K)} + \sum_{i=1}^{N_S} \mathbf{x}_{gi} \mathbf{x}_{gi}^T)^{-1} \left(\sum_{i=1}^{N_S} \mathbf{x}_{gi} y_{ij} \right). \quad (5)$$

The steps for training TSK fuzzy system is summarized in Algorithm 1.

Algorithm 1 TSK Fuzzy System Model

Initialization: Set the number of fuzzy rules K and the regularization parameter λ_1 .

Stage 1: Construct dataset for linear regression

Step 2: Determine the antecedents of the TSK fuzzy system by clustering or other partition techniques to partition the dataset in the input space.

Step 3: Construct the new dataset $\tilde{D} = \{\mathbf{x}_{gi}, \mathbf{y}_i\}$ using (3.a)-(3.c)

Stage 2: Obtain the decision function of the TSK fuzzy system model

Step 4: Obtain the parameters of the TSK fuzzy system using (5) and construct the decision function (3.f).

IV. TRANSDUCTIVE TL AND SSL

In this section, the TL-SSL-TSK model, which integrates TL, SSL with a TSK fuzzy system model, is proposed.

A. Transductive TL

As mentioned before, TL can be used to reduce the discrepancy in data distribution between the training data (source domain) and testing data (target domain). Maximum mean discrepancy (MMD) is used in this paper to measure the

distribution distance between the two domains. By minimizing the MMD, the difference in data distribution between the source and the target domains can be reduced effectively, which makes the testing performance close to the training performance. The effectiveness of TL for EEG signal classification has been demonstrated in [12]. In this paper, the same technique is used to enhance the performance of the TSK fuzzy system.

Given a set of labeled training data $D_S = \{\mathbf{x}_i, \mathbf{y}_i | \mathbf{x}_i \in R^d, \mathbf{y}_i \in R^C, i = 1, \dots, N_S\}$ in the source domain and a set of unlabeled testing data $D_T = \{\mathbf{x}_i | \mathbf{x}_i \in R^d, i = 1, \dots, N_T\}$ in the target domain, the projected squared MMD distance between the source domain and target domain is defined as [12], [18]:

$$\begin{aligned} d(P_{\text{source}}, P_{\text{target}}) &= \text{PMMD}^2 \\ &= \sum_{j=1}^C \left\| \frac{1}{N_S} \sum_{i=1}^{N_S} \mathbf{p}_{g,j}^T \mathbf{x}_{gi,S} - \frac{1}{N_T} \sum_{i=1}^{N_T} \mathbf{p}_{g,j}^T \mathbf{x}_{gi,T} \right\|^2 \\ &= \sum_{j=1}^C \left(\frac{1}{N_S^2} \sum_{i=1}^{N_S} \sum_{j=1}^{N_S} \mathbf{p}_{g,j}^T \mathbf{x}_{gi,S} \mathbf{x}_{gj,S}^T \mathbf{p}_{g,j} \right. \\ &\quad + \frac{1}{N_T^2} \sum_{i=1}^{N_T} \sum_{j=1}^{N_T} \mathbf{p}_{g,j}^T \mathbf{x}_{gi,T} \mathbf{x}_{gj,T}^T \mathbf{p}_{g,j} \\ &\quad \left. - \frac{2}{N_S N_T} \sum_{i=1}^{N_S} \sum_{j=1}^{N_T} \mathbf{p}_{g,j}^T \mathbf{x}_{gi,S} \mathbf{x}_{gj,T}^T \mathbf{p}_{g,j} \right), \quad (6) \end{aligned}$$

where $\mathbf{x}_{gi,S}$ is the i th sample in the source domain (training dataset), $\mathbf{x}_{gi,T}$ is the i th sample in the target domain (testing dataset), and \mathbf{p}_g is an expected projection for the TSK-FS model. Let

$$\begin{aligned} \Omega &= \frac{1}{N_S^2} \mathbf{x}_{g,S} [\mathbf{1}]^{N_S \times N_S} \mathbf{x}_{g,S}^T + \frac{1}{N_T^2} \mathbf{x}_{g,T} [\mathbf{1}]^{N_T \times N_T} \mathbf{x}_{g,T}^T \\ &\quad - \frac{1}{N_S N_T} \mathbf{x}_{g,S} [\mathbf{1}]^{N_S \times N_T} \mathbf{x}_{g,T}^T - \frac{1}{N_S N_T} \mathbf{x}_{g,T} [\mathbf{1}]^{N_T \times N_S} \mathbf{x}_{g,S}^T, \quad (7) \end{aligned}$$

then (6) can be written as

$$d(P_{\text{source}}, P_{\text{target}}) = \sum_{j=1}^C \mathbf{p}_{g,j}^T \Omega \mathbf{p}_{g,j}. \quad (8)$$

B. SSL

For offline classification, SSL can be adopted to further improve the classification performance by using the unlabeled testing data which also contain useful information. One approach to realize this idea is illustrated in Fig. 1. It is based on the assumption that the data within the same class are close to each other.

The above heuristics is used to further improve the performance of our system. Specifically, a novel FCM-like [30] SSL approach is designed for label clustering:

$$\begin{aligned} \min J_{SSL}(\mathbf{U}) &= \sum_{j=1}^C \sum_{i=1}^{N_T} \mu_{ij}^m \left\| \mathbf{p}_{g,j}^T \mathbf{x}_{gi,T} - \theta_j \right\|^2 \\ \text{s.t. } \mu_{ij} &\in [0, 1] \text{ and } \sum_{j=1}^C \mu_{ij} = 1 \quad (9) \end{aligned}$$

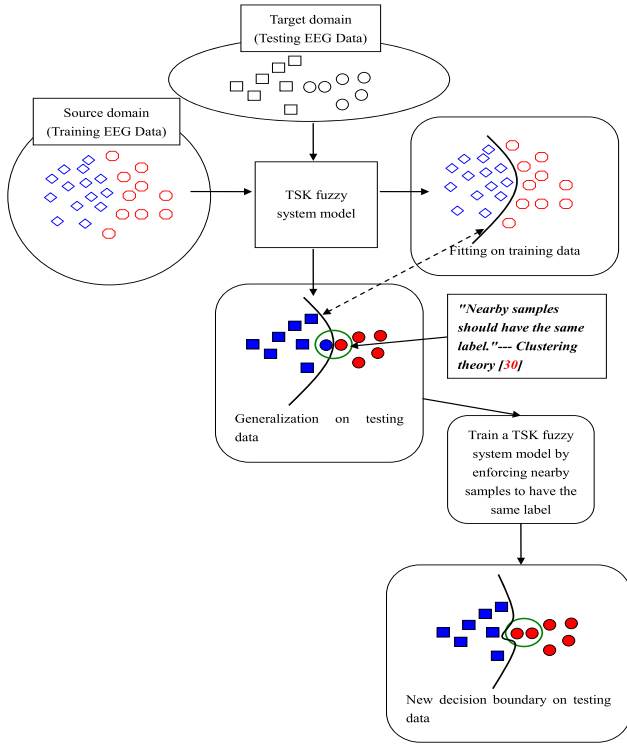


Fig. 1. Illustration of label clustering SSL.

where C is the total number of clusters, N_T is the total number of data of target domain (testing dataset), m is the fuzzy index in FCM, $\mathbf{x}_{gi,T}$ is the i th sample in the target domain, $\mathbf{p}_{g,S}$ is the expected projection of source domain for the TSK fuzzy system model, $\mathbf{U} = [\mu_{ij}]_{C \times N_T}$ is the matrix of fuzzy partition with μ_{ij} denoting the label membership of the i th unlabeled sample of the target domain belonging to the j th cluster, and $\boldsymbol{\theta}_j = [0, \dots, 0, \underset{jth}{1}, 0, \dots, 0]^T$ is a known label vector of the j th cluster ($1 \leq j \leq C$).

C. Learning Algorithms of the TL-SSL-TSK Model

Two learning algorithms are proposed for the TL-SSL-TSK model, which result in two versions of the models, the simple version, namely the *S-TL-SSL-TSK* model, and the advanced version, the *A-TL-SSL-TSK* model.

1) *Learning Algorithm of S-TL-SSL-TSK*: TL and SSL can be integrated with the TSK model using the simple learning objective function:

$$\begin{aligned} \min_{\mathbf{p}_g} J_{S-TL-SSL-TSK} = & \frac{1}{2} \sum_{j=1}^C \sum_{i=1}^{N_S} \left\| \mathbf{p}_{g,j}^T \mathbf{x}_{gi,S} - y_{ij,S} \right\|^2 \\ & + \frac{\lambda_1}{2} \sum_{j=1}^C \mathbf{p}_{g,j}^T \mathbf{p}_{g,j} + \lambda_2 \sum_{j=1}^C \mathbf{p}_{g,j}^T \Omega \mathbf{p}_{g,j} \\ & + \lambda_3 \sum_{j=1}^C \sum_{i=1}^{N_T} \hat{\mu}_{ij}^m \left\| \mathbf{p}_{g,j}^T \mathbf{x}_{gi,T} - \boldsymbol{\theta}_j \right\|^2 \end{aligned} \quad (10)$$

where $\lambda_1 > 0$, $\lambda_2 > 0$, $\lambda_3 > 0$ are the regularization parameters. The first two terms in (10) are used to learn the regularized TSK model based only on the EEG data from

the source domain. The third term is due to transductive TL, and the fourth term due to SSL. For simplicity, the label membership parameter $\hat{\mu}_{ij}$ is set to be a fixed knowledge transfer parameter which directly inherits from the source domain. Similar to classical FCM, $\hat{\mu}_{ij}$ is computed as:

$$\hat{\mu}_{ij} = \frac{\left(\frac{1}{\left\| \mathbf{p}_{g,S}^T \mathbf{x}_{gi,T} - \boldsymbol{\theta}_j \right\|^2} \right)^{\frac{1}{m-1}}}{\sum_{k=1}^C \left(\frac{1}{\left\| \mathbf{p}_{g,S}^T \mathbf{x}_{gi,T} - \boldsymbol{\theta}_k \right\|^2} \right)^{\frac{1}{m-1}}} \quad (11)$$

where the $\mathbf{x}_{gi,T}$ is the i th unlabeled sample in the target domain, $\mathbf{p}_{g,S}$ is an expected projection of the source domain for the TSK-FS model and can be obtained using (5), $\boldsymbol{\theta}_j = [0, \dots, 0, \underset{jth}{1}, 0, \dots, 0]^T$ is a known label vector of the j th cluster.

Let $\hat{\mathbf{U}} = [\hat{\mathbf{U}}_1, \dots, \hat{\mathbf{U}}_C] \in R^{1 \times CN_T}$ be the label membership values for all the unlabeled data where $\hat{\mathbf{U}}_j = [\hat{\mu}_{1j}, \dots, \hat{\mu}_{ij}, \dots, \hat{\mu}_{N_T j}] \in R^{1 \times N_T}$ and $j = 1 \dots C$, $\hat{\mathbf{U}} = \text{diag}(\hat{\mathbf{U}}) \in R^{CN_T \times CN_T}$ be a diagonal matrix of $\hat{\mathbf{U}}$, $\mathbf{V} = [\mathbf{E}, \dots, \mathbf{E}] \in R^{N_T \times CN_T}$ be a transformation matrix where \mathbf{E} is an identity matrix of size N_T , and $\mathbf{Q} = [\mathbf{q}_1, \dots, \mathbf{q}_C] \in R^{C \times CN_T}$ be a transformation matrix where all the values of the j th row of $\mathbf{q}_j \in R^{C \times N_T}$ are 1 and the rest are 0. Then, (10) can be further expressed as:

$$\begin{aligned} \min_{\mathbf{p}_g} J_{S-TL-SSL-TSK} = & \frac{1}{2} \text{tr} \left((\mathbf{p}_g^T \mathbf{x}_{g,S} - \mathbf{y}_S) (\mathbf{p}_g^T \mathbf{x}_{g,S} - \mathbf{y}_S)^T \right) + \frac{\lambda_1}{2} \text{tr} (\mathbf{p}_g^T \mathbf{p}_g) \\ & + \lambda_2 \text{tr} (\mathbf{p}_g^T \Omega \mathbf{p}_g) \\ & + \lambda_3 \text{tr} \left((\mathbf{p}_g^T \mathbf{x}_{g,T} \mathbf{V} - \mathbf{Q}) \hat{\mathbf{U}} (\mathbf{p}_g^T \mathbf{x}_{g,T} \mathbf{V} - \mathbf{Q})^T \right) \end{aligned} \quad (12)$$

where

$$\begin{aligned} \Omega = & \frac{1}{N_T^2} \mathbf{x}_{g,T} [\mathbf{1}]^{N_T \times N_T} \mathbf{x}_{g,T}^T + \frac{1}{N_S^2} \mathbf{x}_{g,S} [\mathbf{1}]^{N_S \times N_S} \mathbf{x}_{g,S}^T \\ & - \frac{1}{N_S N_T} \mathbf{x}_{g,T} [\mathbf{1}]^{N_T \times N_S} \mathbf{x}_{g,S}^T - \frac{1}{N_S N_T} \mathbf{x}_{g,S} [\mathbf{1}]^{N_S \times N_T} \mathbf{x}_{g,T}^T. \end{aligned}$$

The optimal consequent parameters \mathbf{p}_g can be computed by setting the derivatives of $J_{S-TL-SSL-TSK}$ w.r.t. \mathbf{p}_g to zero, and the solution is

$$\begin{aligned} \mathbf{p}_g = & \left(\mathbf{x}_{g,S} \mathbf{x}_{g,S}^T + \lambda_1 \mathbf{I}_{((d+1)*K) \times ((d+1)*K)} \right)^{-1} \\ & + 2\lambda_2 \Omega + 2\lambda_3 \mathbf{x}_{g,T} \mathbf{V} \hat{\mathbf{U}} \mathbf{V}^T \mathbf{x}_{g,T}^T \\ & \times (\mathbf{x}_{g,S} \mathbf{y}^T + 2\lambda_3 \mathbf{x}_{g,T} \mathbf{V} \hat{\mathbf{U}} \mathbf{Q}^T). \end{aligned} \quad (13)$$

The algorithm for S-TL-SSL-TSK is given in Algorithm 2.

Remark: Although the S-TL-SSL-TSK algorithm introduces the transductive TL and SSL mechanism for fuzzy system training, the learning ability of this algorithm can still be further enhanced. Since the label membership parameter $\hat{\mu}_{ij}$ in S-TL-SSL-TSK is a fixed parameter, i.e. directly inheriting from the source domain in step 4 of Algorithm 2, the algorithm is weak in adapting to $\hat{\mu}_{ij}$. In the next subsection, a more adaptive algorithm will be proposed.

Algorithm 2 Learning Algorithm for S-TL-SSL-TSK

Initialization: Set the number of fuzzy rules K , the regularization parameters $\lambda_1, \lambda_2, \lambda_3$, and the fuzzy index m .

Stage 1: Construct dataset for linear regression

- Step 1: Determine the antecedents of the TSK fuzzy system by clustering or other partition techniques to partition the dataset in the input space.
- Step 2: Construct the new training dataset $\tilde{D}_S = \{\mathbf{x}_{g,S}, \mathbf{y}_S\}$ in the source domain and the new testing datasets $\tilde{D}_T = \{\mathbf{x}_{g,T}\}$ by using (3.a)-(3.c).

Stage 2: Obtain the knowledge transfer parameter

- Step 3: Obtain the consequent parameters $\mathbf{p}_{g,S}$ of the source domain using (5).
- Step 4: Obtain the knowledge transfer parameter, i.e. label membership $\hat{\mu}_{ij}$, using (11) with the optimized $\mathbf{p}_{g,S}$;

Stage 3: Generate the S-TL-SSL-TSK model

- Step 5: Obtain the consequent parameters \mathbf{p}_g of the target domain using (13) and get the decision function (3.f) of the S-TL-SSL-TSK model.

2) Learning Algorithm of A-TL-SSL-TSK: To further enhance the abilities of TL and SSL in the proposed TL-SSL-TSK model, a more sophisticated label clustering mechanism is proposed to replace the fourth term in (10):

$$J_{\text{label-clustering}} = \sum_{i=1}^{N_T} \sum_{j=1}^C \left(\eta \mu_{ij}^m + (1 - \eta) \hat{\mu}_{ij}^m \right) \times \left\| \mathbf{p}_g^T \mathbf{x}_{gi,T} - \theta_j \right\|^2, \quad (14)$$

where $\eta \in [0, 1]$ is a trade-off parameter controlling the degree of knowledge transfer between the source domain and the target domain. When $\eta \rightarrow 1$, the knowledge in the target domain, i.e., parameter μ_{ij} , is emphasized. In contrast, when $\eta \rightarrow 0$, the knowledge in the source domain, i.e., parameter $\hat{\mu}_{ij}$, is emphasized.

Substituting (14) into (10), the objective function of A-TL-SSL-TSK is expressed as:

$$\begin{aligned} \min_{\mathbf{p}_g} J_{A-TL-SSL-TSK} &= \frac{1}{2} \sum_{j=1}^C \sum_{i=1}^{N_S} \left\| \mathbf{p}_{g,j}^T \mathbf{x}_{gi,S} - y_{ij,S} \right\|^2 \\ &+ \frac{\lambda_1}{2} \sum_{j=1}^C \mathbf{p}_{g,j}^T \mathbf{p}_{g,j} + \lambda_2 \sum_{j=1}^C \mathbf{p}_{g,j}^T \Omega \mathbf{p}_{g,j} \\ &+ \lambda_3 \sum_{i=1}^{N_T} \sum_{j=1}^C \left(\eta \mu_{ij}^m + (1 - \eta) \hat{\mu}_{ij}^m \right) \left\| \mathbf{p}_g^T \mathbf{x}_{gi,T} - \theta_j \right\|^2 \\ \text{s.t. } \mu_{ij} &\in [0, 1] \text{ and } \sum_{j=1}^C \mu_{ij} = 1 \end{aligned} \quad (15)$$

Similar to (12), (15) can be expressed as:

$$\begin{aligned} \min_{\mathbf{p}_g} J_{A-TL-SSL-TSK} &= \frac{1}{2} \text{tr} \left((\mathbf{p}_g^T \mathbf{x}_{g,S} - \mathbf{y}_S) (\mathbf{p}_g^T \mathbf{x}_{g,S} - \mathbf{y}_S)^T \right) + \frac{\lambda_1}{2} \text{tr} (\mathbf{p}_g^T \mathbf{p}_g) \\ &+ \lambda_2 \text{tr} (\mathbf{p}_g^T \Omega \mathbf{p}_g) + \lambda_3 \text{tr} \left((\mathbf{p}_g^T \mathbf{x}_{g,T} \mathbf{V} - \mathbf{Q}) \right. \\ &\quad \left. \times (\eta \mathbf{U} + (1 - \eta) \hat{\mathbf{U}}) (\mathbf{p}_g^T \mathbf{x}_{g,T} \mathbf{V} - \mathbf{Q})^T \right) \\ \text{s.t. } \mu_{ij} &\in [0, 1] \text{ and } \sum_{j=1}^C \mu_{ij} = 1 \end{aligned} \quad (16)$$

The joint optimization of \mathbf{p}_g and μ_{ij} in (16) makes it non-convex and a closed-form solution is not available. Thus, an iterative optimization method [15], [32] is adopted in this paper, which contains the two steps below.

i) Step 1: Compute \mathbf{p}_g :

When the parameter μ_{ij} is fixed, i.e., $\hat{\mathbf{U}}$ is fixed, the minimization of $J_{A-TL-SSL-TSK}$ can be computed by setting the derivatives of (16) w.r.t. \mathbf{p}_g to zero, and we obtain:

$$\mathbf{p}_g = \left(\mathbf{I}_{((d+1)*K) \times ((d+1)*K)} + \lambda_1 \mathbf{x}_{g,S} \mathbf{x}_{g,S}^T + 2\lambda_2 \Omega \right)^{-1} \left(\begin{aligned} &+ 2\lambda_3 \mathbf{x}_{g,T} \mathbf{V} (\eta \mathbf{U} + (1 - \eta) \hat{\mathbf{U}}) \mathbf{V}^T \mathbf{x}_{g,T}^T \\ &\times \left(\begin{aligned} &\lambda_1 \mathbf{x}_{g,S} \mathbf{y}^T \\ &+ 2\lambda_3 \mathbf{x}_{g,T} \mathbf{V} (\eta \mathbf{U} + (1 - \eta) \hat{\mathbf{U}}) \mathbf{Q}^T \end{aligned} \right) \end{aligned} \right) \quad (17)$$

ii) Step 2: Compute μ_{ij} :

When the parameter \mathbf{p}_g is fixed, by minimizing (17) using the Lagrangian method, the following update equation for the label fuzzy membership μ_{ij} is obtained.

$$\mu_{ij} = \frac{\left(\frac{1}{\left\| \mathbf{p}_g^T \mathbf{x}_{gi,T} - \theta_j \right\|^2} \right)^{\frac{1}{m-1}}}{\sum_{k=1}^C \left(\frac{1}{\left\| \mathbf{p}_g^T \mathbf{x}_{gi,T} - \theta_k \right\|^2} \right)^{\frac{1}{m-1}}} \quad (18)$$

The complete learning algorithm for A-TL-SSL-TSK is given in Algorithm 3.

V. EXPERIMENTAL STUDY

In this section, the two proposed models, i.e., S-TL-SSL-TSK and A-TL-SSL-TSK, are evaluated by performing two-class classification between EEG signals of healthy subjects and that of epileptic subjects captured during seizure. In addition, they are compared with six classical non-TL-based methods and four TL-based or SSL-based methods, as shown in Table I.

To ensure fair comparison, the same EEG data and feature extraction methods are used for all the algorithms, as in our previous work [12]. The details of the experimental settings and the scenarios of TL are described below.

A. Experimental Settings

In our experiments, all the algorithms were implemented using MATLAB on a computer with Intel Core i5-3317U 1.70 GHz CPU and 16GB RAM. The experimental settings

Algorithm 3 Learning Algorithm for the A-TL-SSL-TSK Model

Initialization: Set the number of fuzzy rules K , regularization parameters $\lambda_1, \lambda_2, \lambda_3$, transfer parameter η , convergence threshold ε , fuzzy index m , maximum number of iterations T . Initialize the fuzzy partition $\mu_{ij}^{(s)}$ and set the iterative index $l = 1$

Stage 1: Construct dataset for linear regression

- Step 1: Determine the antecedents of TSK fuzzy system by clustering or other partition techniques to partition the dataset in the input space.
- Step 2: Construct the new training dataset $\tilde{D}_s = \{\mathbf{x}_{g,s}, \mathbf{y}_s\}$ of source domain and the new testing datasets $\tilde{D}_t = \{\mathbf{x}_{g,t}\}$ by using (3.a)-(3.c).

Stage 2: Obtain the knowledge transfer parameter

- Step 3: Obtain the consequent parameters $\mathbf{p}_{g,s}$ of the source domain by (5).
- Step 4: Obtain the knowledge transfer parameter, i.e., label membership $\hat{\mu}_{ij}$, using (11) and the optimized $\mathbf{p}_{g,s}$.

Stage 3: Generate the A-TL-SSL-TSK model

- Step 5: Compute the consequent parameter $\mathbf{p}_g^{(l+1)}$ using (17) with $\mu_{ij}^{(l)}$
- Step 6: Compute the label fuzzy membership $\mu_{ij}^{(l+1)}$ using (18) with $\mathbf{p}_g^{(l+1)}$;
- Step 7: If $|U^{(l+1)} - U^{(l)}| < \varepsilon$ or the number of iterations $l > T$, terminate and output the consequent parameter $\mathbf{p}_g^{(l+1)}$ of the A-TL-SSL-TSK model; otherwise, set $l = l + 1$ and go to step 5.
- Step 8: Obtain the optimized consequent parameters \mathbf{p}_g of the target domain by following steps 5 to 7 and get the decision function (3.f) of the A-TL-SSL-TSK model.

TABLE I
EXPERIMENTAL SETTINGS

	Non-TL-based methods	TL-based or SSL-based methods
Methods for comparison	1. LDA [5,8,10] 2. DT [9] 3. NB [7,9] 4. NM [7] 5. SVM [6] 6. TSK	1. TSVM [33] 2. S4VM [34] 3. LMPROJ [18] 4. GTL2 [35] 5. S-TL-SSL-TSK 6. A-TL-SSL-TSK
EEG data	The EEG data used in this study are the same as those in [12], and can be downloaded from http://epileptologie-bonn.de/cms/front_content.php?idcat=193&lang=3&changelang=3 [41]. It contains five groups of data (Groups A to E) and each group contains 100 single channel EEG segments of 23.6s duration. The sampling rate of all the datasets was 173.6 Hz. Table II gives a detailed description of the five groups. Fig. 2 shows some typical EEG signals in each group.	
Feature extraction methods	1. Wavelet packet decomposition (WPD) 2. Short time Fourier transform (STFT) 3. Kernel principal component analysis (KPCA)	
Performance evaluation measures	1. Accuracy: Number of correctly predicted testing data divided by the number of the total testing data. 2. Friedman test combined with Holm's post hoc test [36,37].	
Method-specific settings	1. For LDA, DT, NB, NM, SVM and LMPROJ methods, we adopted the same experimental setting in [12]. 2. For TSVM, S4VM and GTL2 methods, we adopted the same experimental setting in [33], [34] and [35] respectively. 3. For TSK, S-TL-SSL-TSK and A-TL-SSL-TSK, the number of fuzzy rules was selected from $\{5, 10, 15, 20, 25, 30\}$, the regularization parameters λ_1, λ_2 and λ_3 were selected from $\{10^{-3}, 10^{-2}, \dots, 10^2, 10^3\}$, the transfer balance parameter η was selected from $\{0, 0.1, 0.2, 0.3, \dots, 0.9, 1\}$, and the fuzzy index m was selected from $\{1.1, 1.5, 2, 2.5\}$. Five-fold cross-validation on the training data was applied for all the methods.	

are summarized in Table I. Note that TSVM and S4VM are SSL-based methods, where the unlabeled EEG data in the target domain are used for learning. LMPROJ and GTL2 are TL-based methods.

B. TL Scenarios for Epileptic EEG Recognition

The two TL scenarios used in our previous work [12] were adopted in this study. In the first scenario, the data distributions of the source and the target domain were the same, as shown in the first part of Table III. In the second scenario, the data distributions were different, as shown in the second part of Table III. More details of these two scenarios can be found in [12, Sec. 4.1.2].

C. Experimental Results and Discussions

1) **Recognition Performance Analysis:** The following arrangements were made to achieve comprehensive

comparison. Three different feature extraction methods were used, i.e., WPD, STFT, and KPCA. For each method, we compared S-TL-SSL-TSK and A-TL-SSL-TSK with six non-TL-based methods and four sets of features. The classification results are shown in Tables IV-VI and the findings below are drawn.

(1) Among the six non-TL-based methods (LDA, DT, NB, NM, SVM and TSK), TSK showed the best overall performance. The results indicate that TSK is an effective approach for epileptic EEG recognition. In addition, it has better interpretability than other black-box methods like SVM.

(2) For Datasets D1 and D2, where the source and the target domains had the same data distribution, most non-TL-based methods achieved high accuracy. However, for Datasets D3-D6, where the source and the target domains had different data distributions, their performance deteriorated significantly. This is because the data distributions of the training and testing

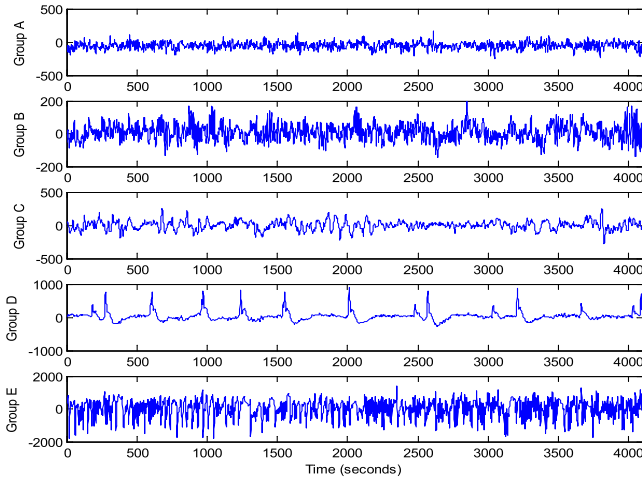


Fig. 2. Typical EEG signals in Groups A-E.

TABLE II
DESCRIPTION OF THE EEG DATA

Subjects	Groups	Size of groups	Descriptions of datasets
Healthy	A	100	EEG signals measured from healthy people with eyes open
	B	100	EEG signals measured from healthy people with eyes closed
Epileptic	C	100	EEG signals obtained in the hippocampal formation of the opposite hemisphere of the brain during seizure free intervals
	D	100	EEG signals obtained from within the epileptogenic zone during seizure free intervals
	E	100	EEG signals measured during seizure

datasets were inappropriately assumed to be the same, and hence they were not able to adapt to the new data of different distribution in the target domain.

(3) Compared with the six classical non-TL-based methods, the six TL-based or SSL-based methods achieved higher accuracy consistently. These results indicate that TL and SSL can indeed be used to improve the classification performance of epileptic EEG recognition.

(4) Among the six TL-based or SSL-based methods, S-TL-SSL-TSK and A-TL-SSL-TSK showed the best overall recognition performance, especially for Datasets D3-D6. This is because TSVM and S4VM only used SSL, and LMPROJ and GTL2 only used TL, whereas the proposed S-TL-SSL-TSK and A-TL-SSL-TSK used both, i.e., S-TL-SSL-TSK and A-TL-SSL-TSK explicitly reduced the discrepancy in data distribution between the source and the

target domains, and made use of the information contained in the unlabeled EEG samples of the target domain at the same time.

(5) A-TL-SSL-TSK almost always outperformed S-TL-SSL-TSK. This is expected, since A-TL-SSL-TSK employed a more flexible TL mechanism and was tuned using more parameters. However, the computational cost of A-TL-SSL-TSK is higher. So, the choice between S-TL-SSL-TSK and A-TL-SSL-TSK is a tradeoff between computational cost and classification accuracy.

To evaluate whether the performance difference among the algorithms were statistically significant, Friedman test [36], [37] and the Holm post hoc test [36], [37] were performed. Friedman test was used to compute the average ranks of the different methods, and to evaluate whether statistically significant difference existed among them. The null hypothesis was that there was no statistically significant difference. If the p -value was smaller than 0.05, the null hypothesis was rejected. The Holm post hoc test was also performed to verify if there was statistically significant difference between the control approach, i.e., the one achieving the best Friedman rank, and the other approaches.

We first compared S-TL-SSL-TSK with all the other methods except A-TL-SSL-TSK, and then A-TL-SSL-TSK with all the other methods except S-TL-SSL-TSK. The results are summarized in Tables VII and VIII. The results of the Friedman test indicate that there was statistically significant difference in accuracy between the two proposed methods and the other ten methods. The Holm's post hoc test shows that S-TL-SSL-TSK and A-TL-TSK-FS significantly outperformed all the six non-TL-based methods and TSVM, but not so for GTL2, S4VM and LMPROJ. Although the increase in performance of our proposed methods over GTL2, S4VM and LMPROJ was not statistically significant, they improved the interpretability which is important for medical diagnostics.

In summary, the experimental results demonstrate that S-TL-SSL-TSK and A-TL-SSL-TSK are suitable for epileptic EEG recognition: their classification performance is comparable to or even better than many state-of-the-art classification algorithms, and they have better interpretability.

2) *Model Interpretability Analysis*: The interpretability of A-TL-SSL-TSK is analyzed here to demonstrate the advantage of the proposed methods. A model constructed by A-TL-SSL-TSK using the Dataset D1 is shown in Table IX, which result in five fuzzy rules.

In Table IX, the parameters involved in the fuzzy sets of five fuzzy rules are given. Fig. 3 presents the corresponding membership functions (MFs) of each fuzzy set obtained for all the fuzzy rules, where each MF corresponds to a fuzzy linguistic description, such as "the energy of a band of EEG signal is Low (or *A little low, Medium, A little high, High*). The given linguistic description is only a possible explanation for the IF-Part of fuzzy rule, since different medical experts may use different linguistic descriptions for the same rule.

To provide further explanation, take the rules in the second row of Fig. 3 as an example. According to the antecedent parameters (centers \mathbf{c} and variance δ of Band 1 in Fig. 3, i.e., (3.58, 1.87) for 1st fuzzy rule, (4.27, 2.87) for 2nd fuzzy

TABLE III
DETAILS OF THE TL SCENARIOS FOR EPILEPTIC EEG RECOGNITION

Scenario	Datasets	Source domain (training dataset)	Target domain (testing dataset)	Number of samples in the source domain	Number of samples in the target domain
Scenario 1: Same distribution	D1	Groups A and E	Groups A and E	150	50
	D2	Groups A, B and E	Groups A, B and E	150	50
Scenario 2: Different distribution	D3	Groups A and E	Groups A and C	50	50
	D4	Groups A and E	Groups A and D	50	50
	D5	Groups A, C and E	Groups B, C and E	75	75
	D6	Groups A, D and E	Groups B, D and E	75	75

TABLE IV
PERFORMANCE COMPARISON OF THE CLASSIFIERS USING WPD FEATURES

Part A: Non-TL methods						
Datasets	LDA	DT	NB	NM	SVM	TSK
D1	0.922±0.012	0.887±0.01	0.851±0.006	0.798±0.008	0.918±0.004	0.914±0.025
D2	0.927±0.087	0.936±0.008	0.922±0.012	0.833±0.02	0.92±0.001	0.928±0.009
D3	0.544±0.007	0.825±0.02	0.527±0.007	0.425±0.004	0.824±0.06	0.826±0.056
D4	0.561±0.009	0.808±0.02	0.573±0.008	0.469±0.01	0.816±0.044	0.812±0.068
D5	0.772±0.006	0.802±0.018	0.559±0.005	0.515±0.008	0.807±0.03	0.812±0.054
D6	0.739±0.01	0.778±0.07	0.622±0.026	0.535±0.009	0.81±0.06	0.824±0.038
Part B: TL methods						
Datasets	TSVM	S4VM	LMPROJ	GTL2	S-TL-SSL-TSK	A-TL-SSL-TSK
D1	0.924±0.009	0.967±0.038	0.937±0.004	0.931±0.022	0.950±0.010	0.958±0.011
D2	0.929±0.007	0.965±0.018	0.936±0.001	0.945±0.036	0.957±0.009	0.961±0.006
D3	0.843±0.034	0.856±0.033	0.941±0.011	0.929±0.049	0.953±0.007	0.957±0.005
D4	0.837±0.025	0.860±0.025	0.945±0.008	0.917±0.067	0.960±0.012	0.966±0.008
D5	0.821±0.039	0.829±0.056	0.925±0.008	0.939±0.048	0.948±0.017	0.956±0.016
D6	0.845±0.041	0.868±0.060	0.945±0.005	0.922±0.051	0.966±0.006	0.968±0.007

TABLE V
PERFORMANCE COMPARISON OF THE CLASSIFIERS USING STFT FEATURES

Datasets	Part A: Non-TL methods					
	LDA	DT	NB	NM	SVM	TSK
D1	0.983±0.036	0.994±0.003	0.947±0.005	0.990±0.019	0.988±0.003	0.988±0.014
D2	0.981±0	0.951±0.02	0.933±0.017	0.890±0.036	0.994±0.002	0.992±0.011
D3	0.536±0.03	0.62±0.09	0.53±0.022	0.495±0.003	0.51±0.015	0.564±0.066
D4	0.565±0.015	0.675±0.05	0.632±0.003	0.537±0.007	0.562±0.031	0.586±0.057
D5	0.622±0.02	0.476±0.04	0.417±0.043	0.483±0.02	0.864±0.02	0.873±0.036
D6	0.601±0.03	0.46±0.02	0.375±0.022	0.484±0.018	0.874±0.054	0.876±0.073
Datasets	Part B: TL methods					
	TSVM	S4VM	LMPROJ	GTL2	S-TL-SSL-TSK	A-TL-SSL-TSK
D1	0.992±0.010	0.996±0.008	0.977±0.001	0.992±0.026	0.994±0.013	0.994±0.009
D2	0.998±0.004	0.994±0.009	0.994±0.001	0.993±0.057	0.994±0.006	0.996±0.006
D3	0.526±0.036	0.860±0.036	0.945±0.008	0.910±0.027	0.948±0.007	0.963±0.009
D4	0.598±0.072	0.872±0.027	0.938±0.01	0.940±0.018	0.957±0.005	0.957±0.003
D5	0.876±0.034	0.884±0.037	0.952±0.008	0.931±0.049	0.960±0.018	0.967±0.012
D6	0.891±0.075	0.905±0.039	0.949±0.01	0.924±0.039	0.953±0.025	0.974±0.036

rule, (5.11, 2.06) for 3rd fuzzy rule, (1.66, 2.33) for 4th fuzzy rule, and (8.34, 2.52) for 5th fuzzy rule, five MFs can be generated to represent this feature (Band 1). In addition, these

five MFs can be linguistically expressed as “A little low”, “Medium”, “A little high”, “Low”, and “High” in ascending order of the values of the centers. Similarly, the other features

TABLE VI
PERFORMANCE COMPARISON OF THE CLASSIFIERS USING KPCA FEATURES

Part A: Non-TL methods						
Datasets	LDA	DT	NB	NM	SVM	TSK
D1	0.882±0.058	0.932±0.017	0.82±0.075	0.747±0.064	0.92±0.02	0.936±0.038
D2	0.827±0.065	0.86±0.026	0.682±0.094	0.649±0.041	0.91±0.011	0.924±0.026
D3	0.741±0.09	0.795±0.07	0.628±0.05	0.673±0.11	0.79±0.02	0.752±0.033
D4	0.765±0.09	0.944±0.06	0.625±0.13	0.721±0.12	0.82±0.04	0.792±0.028
D5	0.46±0.061	0.739±0.043	0.491±0.3	0.447±0.06	0.710±0.02	0.766±0.051
D6	0.53±0.035	0.711±0.02	0.641±0.10	0.487±0.04	0.721±0.02	0.777±0.012
Part B: TL methods						
Datasets	TSVM	S4VM	LMPROJ	GTL2	S-TL-SSL-TSK	A-TL-SSL-TSK
D1	0.942±0.035	0.984±0.021	0.958±0.01	0.943±0.023	0.984±0.015	0.984±0.012
D2	0.924±0.022	0.971±0.023	0.948±0.004	0.906±0.026	0.958±0.014	0.966±0.013
D3	0.862±0.048	0.908±0.021	0.949±0.05	0.930±0.030	0.952±0.027	0.957±0.029
D4	0.894±0.059	0.918±0.016	0.963±0.009	0.940±0.039	0.978±0.022	0.984±0.012
D5	0.773±0.072	0.842±0.076	0.948±0.015	0.956±0.030	0.962±0.047	0.978±0.018
D6	0.764±0.067	0.891±0.043	0.95±0.008	0.946±0.021	0.958±0.036	0.965±0.025

TABLE VII
RESULTS OF FRIEDMAN TEST ON ALL THE DATASETS IN TERMS OF AVERAGE PERFORMANCE ($\alpha = 0.05$)

Part A: Friedman Test for S-TL-TSK-FS				Part B: Friedman Test for A-TL-TSK-FS			
Algorithms	Friedman Rank	p-value	Hypothesis	Algorithms	Friedman Rank	p-value	Hypothesis
LDA	8.6667	0	Rejected	LDA	8.6667	0	Rejected
DT	6.9444			DT	6.9444		
NB	9.7222			NB	9.7222		
NM	10.3889			NM	10.3889		
SVM	7.3889			SVM	7.4167		
TSK	6.5556			TSK	6.5556		
TSVM	5.2222			TSVM	5.2222		
S4VM	3.2222			S4VM	3.25		
LMPROJ	3			LMPROJ	3.0278		
GTL2	3.4722			GTL2	3.4722		
S-TL-SSL-TSK	1.4167			A-TL-SSL-TSK	1.3333		

can also be divided into these five classes. Finally, with the linguistic expression of the *IF-Part* of the fuzzy rule and the corresponding linear function of the *THEN-Part*, the five fuzzy rules that are generated based on the WPD features can be described linguistically as follows:

The 1st Fuzzy Rule:

IF the energy of the EEG signal in the frequency band 1 is A little low,
and the energy of the EEG signal in the frequency band 2 is A little high,
and the energy of the EEG signal in the frequency band 3 is A little high,
and the energy of the EEG signal in the frequency band 4 is A little high,
and the energy of the EEG signal in the frequency band 5 is A little low,

and the energy of the EEG signal in the frequency band 6 is A little low,

THEN this rule gives the decision values of the two outputs with the following formula:

The 2nd Fuzzy Rule:

IF the energy of the EEG signal in the frequency band 1 is Medium,
and the energy of the EEG signal in the frequency band 2 is Medium,
and the energy of the EEG signal in the frequency band 3 is Medium,
and the energy of the EEG signal in the frequency band 4 is A little low,
and the energy of the EEG signal in the frequency band 5 is Medium,

$$f^1(\mathbf{x}) = \begin{bmatrix} 0.2714 + 0.4287x_1 - 0.5325x_2 + 0.1676x_3 - 0.1119x_4 + 0.0872x_5 + 0.0031x_6, \\ -0.2616 - 0.4189x_1 + 0.5427x_2 - 0.1576x_3 + 0.1219x_4 - 0.0772x_5 - 0.0025x_6 \end{bmatrix}.$$

$$f^2(\mathbf{x}) = \begin{bmatrix} 0.1024 + 0.2909x_1 - 0.2746x_2 - 0.0503x_3 + 0.1071x_4 - 0.0213x_5 + 0.0015x_6, \\ -0.0928 - 0.2813x_1 + 0.2849x_2 + 0.0603x_3 - 0.0971x_4 + 0.0313x_5 - 0.0009x_6 \end{bmatrix}.$$

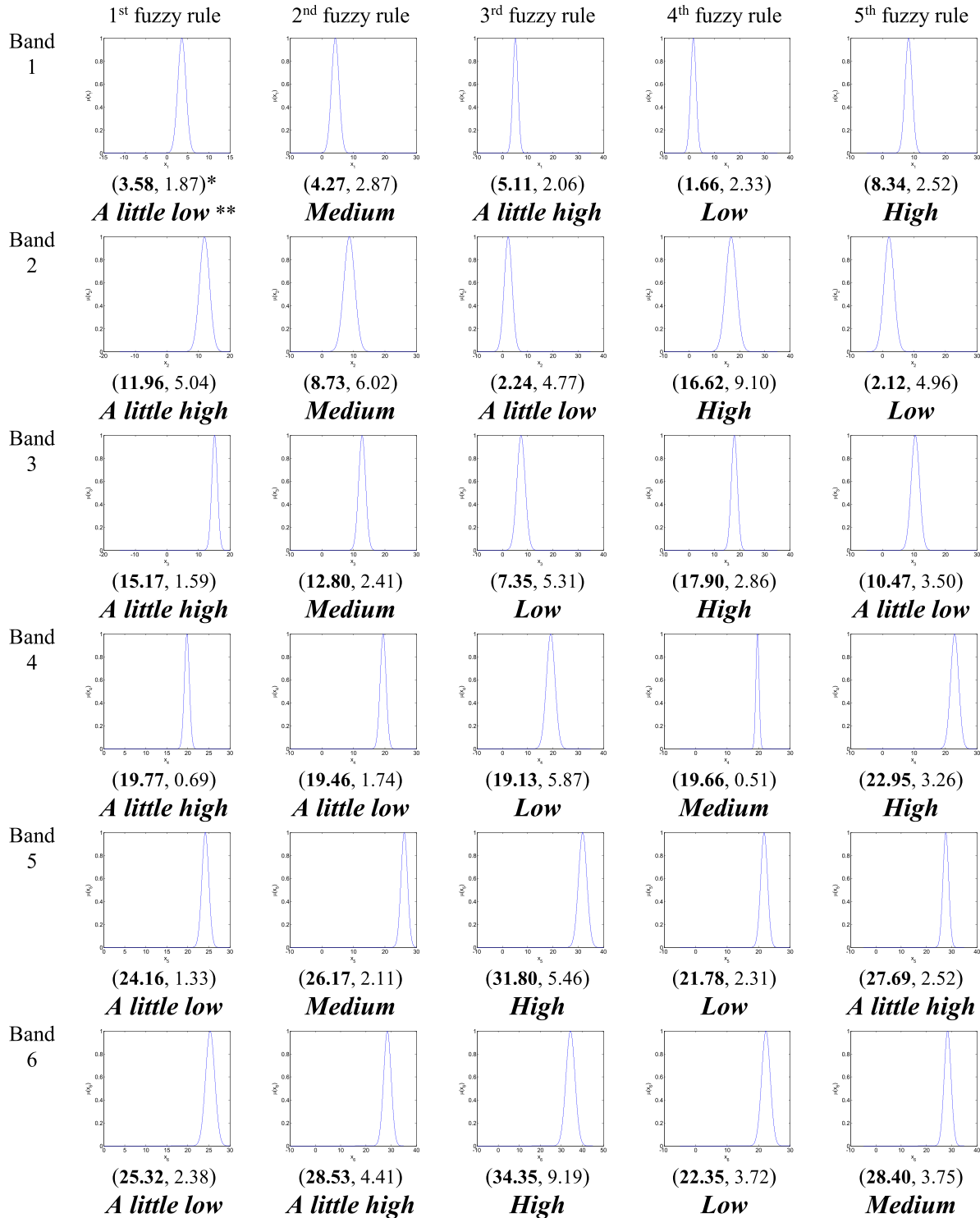


Fig. 3. The membership functions and the possible linguistic explanation of each fuzzy subset in the antecedent of the fuzzy rules of the TSK fuzzy system. The system is obtained by the A-TL-SSL-TSK based on the WPD features. * The antecedent parameter (c_1^1, δ_1^1) of Band 1 (first dimension of the data) of the first fuzzy rule. ** A possible explanation for the fuzzy set obtained.

and the energy of the EEG signal in the frequency band 6 is
A little high,

THEN this rule gives the decision values of the two outputs with the following formula:

The 3rd Fuzzy Rule:

IF the energy of the EEG signal in the frequency band 1 is
A little high,

and the energy of the EEG signal in the frequency band 2 is
A little low,

and the energy of the EEG signal in the frequency band 3 is
Low,

and the energy of the EEG signal in the frequency band 4 is
Low,

and the energy of the EEG signal in the frequency band 5 is

TABLE VIII

HOLM'S POST HOC COMPARISON OVER THE RESULTS OF FRIEDMAN TEST ON ALL THE DATASETS
IN TERMS OF AVERAGE PERFORMANCE ($\alpha = 0.05$)

Part A: Holm's Post Hoc Comparison for S-TT-TSK-FS					
i	Algorithms	$z = (R_0 - R_i) / SE$	p	$Holm = \alpha / i$	Hypothesis
10	NM	8.11568	0	0.005	Rejected
9	NB	7.512658	0	0.005556	Rejected
8	LDA	6.557872	0	0.00625	Rejected
7	SVM	5.402078	0	0.007143	Rejected
6	DT	5.000063	0.000001	0.008333	Rejected
5	TSK	4.6483	0.000003	0.01	Rejected
4	TSVM	3.442255	0.000577	0.0125	Rejected
3	GTL2	1.85932	0.062982	0.016667	Not rejected
2	S4VM	1.633186	0.10243	0.025	Not rejected
1	LMPROJ	1.432179	0.152093	0.05	Not rejected
Part B: Holm's Post Hoc Comparison for A-TT-TSK-FS					
i	Algorithms	$z = (R_0 - R_i) / SE$	p	$Holm = \alpha / i$	Hypothesis
10	NM	8.191058	0	0.005	Rejected
9	NB	7.588036	0	0.005556	Rejected
8	LDA	6.63325	0	0.00625	Rejected
7	SVM	5.502582	0	0.007143	Rejected
6	DT	5.075441	0	0.008333	Rejected
5	TSK	4.723678	0.000002	0.01	Rejected
4	TSVM	3.517632	0.000435	0.0125	Rejected
3	GTL2	1.934698	0.053027	0.016667	Not rejected
2	S4VM	1.73369	0.082973	0.025	Not rejected
1	LMPROJ	1.532683	0.125354	0.05	Not rejected

TABLE IX

AN A-TL-SSL-TSK MODEL WITH FIVE RULES TRAINED USING THE DATASET D1 WITH WPD FEATURES

Fuzzy rules base		
TSK fuzzy rule R^k :		
IF x_1 is $A_1^k(c_1^k, \delta_1^k) \wedge x_2$ is $A_2^k(c_2^k, \delta_2^k) \wedge \dots \wedge x_d$ is $A_d^k(c_d^k, \delta_d^k)$, THEN $f^k(\mathbf{x}) = p_0^k + p_1^k x_1 + \dots + p_d^k x_d$.		
No. of rules	Antecedent parameters (Gaussian membership function parameters)	Consequent parameters (linear function parameters)
k	$\mathbf{c}^k = (c_1^k, \dots, c_d^k)^T, \mathbf{\delta}^k = (\delta_1^k, \dots, \delta_d^k)^T$	$\mathbf{p}_k = (p_{k0}, p_{k1}, \dots, p_{kd})^T$
1	$\mathbf{c}^1 = [3.58, 11.96, 15.17, 19.77, 24.16, 25.32],$ $\mathbf{\delta}^1 = [1.87, 5.04, 1.59, 0.69, 1.33, 2.38]$	$\mathbf{p}_1 = [0.2714, 0.4287, -0.5325, 0.1676, -0.1119, 0.0872, 0.0031;$ $-0.2616, -0.4189, 0.5427, -0.1576, 0.1219, -0.0772, -0.0025]$
2	$\mathbf{c}^2 = [4.27, 8.73, 12.80, 19.46, 26.17, 28.53],$ $\mathbf{\delta}^2 = [2.87, 6.02, 2.41, 1.74, 2.11, 4.41]$	$\mathbf{p}_2 = [0.1024, 0.2909, -0.2746, -0.0503, 0.1071, -0.0213, 0.0015;$ $-0.0928, -0.2813, 0.2849, 0.0603, -0.0971, 0.0313, -0.0009]$
3	$\mathbf{c}^3 = [5.11, 2.24, 7.35, 19.13, 31.80, 34.35],$ $\mathbf{\delta}^3 = [2.06, 4.77, 5.31, 5.87, 5.46, 9.19]$	$\mathbf{p}_3 = [0.0569, -0.0160, -0.0416, -0.0115, -0.0264, 0.0326, -6.04e-05;$ $-0.0499, 0.0227, 0.0547, 0.0215, 0.0363, -0.0226, 0.0006]$
4	$\mathbf{c}^4 = [1.66, 16.62, 17.90, 19.66, 21.78, 22.35],$ $\mathbf{\delta}^4 = [2.33, 9.10, 2.86, 0.51, 2.31, 3.72]$	$\mathbf{p}_4 = [-0.0159, 0.2942, -0.2838, -0.0550, 0.0895, 0.0046, 0.0003;$ $0.0257, -0.2844, 0.2940, 0.0648, -0.0793, 0.0052, 0.0002]$
5	$\mathbf{c}^5 = [8.34, 2.12, 10.47, 22.95, 27.69, 28.40],$ $\mathbf{\delta}^5 = [2.52, 4.96, 3.50, 3.26, 2.52, 3.75]$	$\mathbf{p}_5 = [-0.0195, -0.0178, 0.0161, 0.0021, -0.0106, 0.0097, -0.0002;$ $0.0266, 0.0249, -0.0032, 0.0078, 0.0205, 0.0003, 0.0007]$

High,

and the energy of the EEG signal in the frequency band 6 is

High,

THEN this rule gives the decision values of the two outputs with the following formula:

The 4th Fuzzy Rule:

IF the energy of the EEG signal in the frequency band 1 is

Low,

and the energy of the EEG signal in the frequency band 2 is

High,

and the energy of the EEG signal in the frequency band 3 is

High,

and the energy of the EEG signal in the frequency band 4 is

Medium,

and the energy of the EEG signal in the frequency band 5 is

Low,

and the energy of the EEG signal in the frequency band 6 is

Low,

THEN this rule gives the decision values of the two outputs with the following formula:

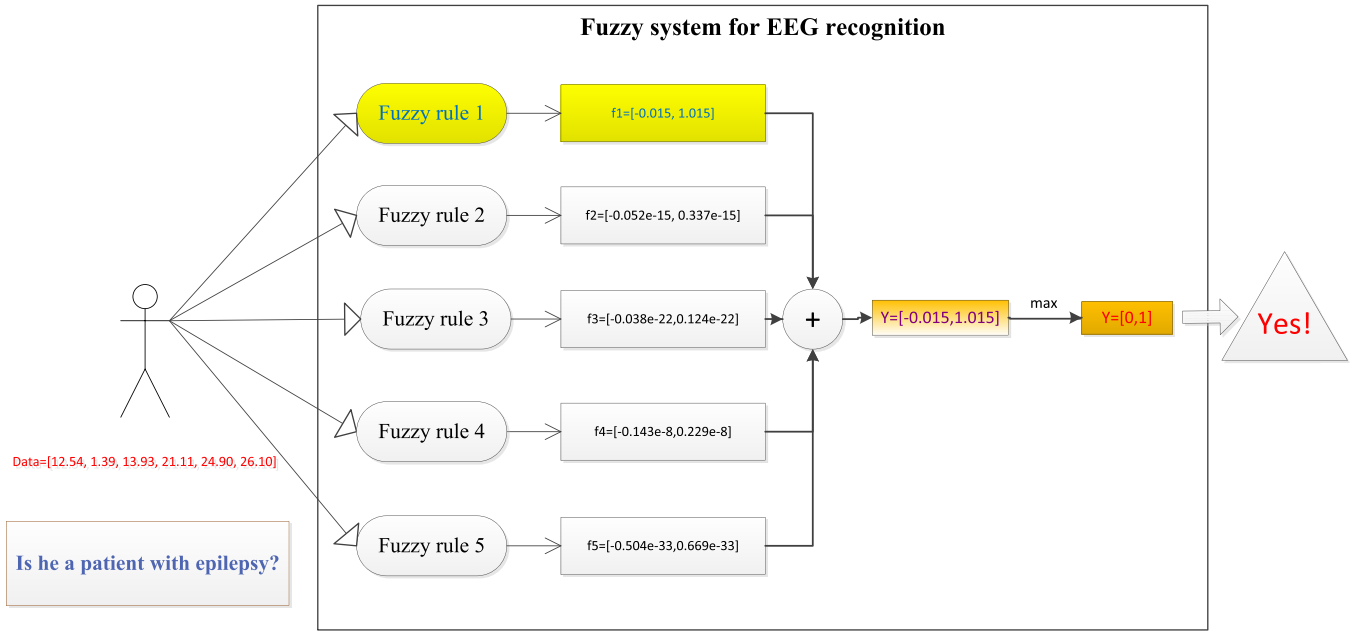


Fig. 4. An example showing the identification of epileptic patient using the fuzzy rules generated and the fuzzy system, where ‘+’ denotes the combination operation and ‘max’ denotes the operation that sets the maximal element in Y to 1 and the others to 0.

The 5th Fuzzy Rule:

*IF the energy of the EEG signal in the frequency band 1 is High,
and the energy of the EEG signal in the frequency band 2 is Low,
and the energy of the EEG signal in the frequency band 3 is A little low,
and the energy of the EEG signal in the frequency band 4 is High,
and the energy of the EEG signal in the frequency band 5 is A little high,
and the energy of the EEG signal in the frequency band 6 is Medium,*

THEN this rule gives the decision values of the two outputs with the following formula:

In a similar way, the fuzzy systems that are learned based on the STFT features and the KPCA features can be interpreted accordingly.

An example is given in Fig. 4 to further explain the usage and the importance of the rules generated by the proposed method. In Fig. 4, the features of the original EEG signals of a patient, extracted by WPD, are used for diagnosis based on the trained A-TL-SSL-TSK fuzzy system. A vector is used to encode the output of the system, with [1, 0] indicating

the control (i.e., healthy people) and [0, 1] indicating the epileptic patient. Using Eq.(3.f), the proposed A-TL-SSL-TSK fuzzy system yields $Y = [-0.015, 1.015]$. According to the “winner takes all” criterion, we further obtain the final output $Y = [0, 1]$, which indicates an epileptic patient. It can be seen from the figure that the absolute values of the components in Fuzzy rule 1 ($f1 = [-0.015, 1.015]$) is much closer to [0, 1] than those in other fuzzy rules, which implies that Fuzzy rule 1 in Fig.4 takes a predominant role in the whole identification process and thus the final decision is primarily determined by this rule.

The above analysis illustrates that the A-TL-SSL-TSK fuzzy system model is an interpretative model for identifying epileptic patient using the fuzzy rules generated.

3) Computational Complexity: In this subsection, the computational complexity of the fuzzy systems trained by the proposed S-TL-SSL-TSK and the A-TL-SSL-TSK algorithms were compared. The running time of the two algorithms on dataset D1 is reported in Table X and the following observations are made.

1) The average training time of the proposed A-TL-SSL-TSK was nearly 10 times longer than that of the S-TL-SSL-TSK since the former contained more model parameters than the latter.

$$f^3(\mathbf{x}) = \begin{bmatrix} 0.0569 - 0.0160x_1 - 0.0416x_2 - 0.0115x_3 - 0.0264x_4 + 0.0326x_5 - 6.04e - 5x_6, \\ -0.0499 + 0.0227x_1 + 0.0547x_2 + 0.0215x_3 + 0.0363x_4 - 0.0226x_5 + 0.0006x_6 \end{bmatrix}.$$

$$f^4(\mathbf{x}) = \begin{bmatrix} -0.0159 + 0.2942x_1 - 0.2838x_2 - 0.0550x_3 + 0.0895x_4 + 0.0046x_5 + 0.0003x_6, \\ 0.0257 - 0.2844x_1 + 0.2940x_2 + 0.0648x_3 - 0.0793x_4 + 0.0052x_5 + 0.0002x_6 \end{bmatrix}.$$

$$f^5(\mathbf{x}) = \begin{bmatrix} -0.0195 - 0.0178x_1 + 0.0161x_2 + 0.0021x_3 - 0.0106x_4 + 0.0097x_5 - 0.0002x_6, \\ 0.0266 + 0.0249x_1 - 0.0032x_2 + 0.0078x_3 + 0.0205x_4 + 0.0003x_5 + 0.0007x_6 \end{bmatrix}.$$

TABLE X
COMPUTATIONAL COMPLEXITY OF THE TL-SSL-TSK MODEL TRAINED BY THE TWO PROPOSED ALGORITHMS ON DATASET D1

Feature extraction Method	Algorithms	Index (Second)		
		Average training time	Average testing time	Real time* (One sample)
WPD	S-TL-SSL-TSK	1.85	1.08e-05	(0.0852+1.56e-07)
	A-TL-SSL-TSK	22.19	1.32e-05	(0.0822+1.69e-07)
STFT	S-TL-SSL-TSK	1.63	1.56e-05	(0.1289+1.56e-07)
	A-TL-SSL-TSK	18.49	1.20e-05	(0.1316+1.44e-07)
KPCA	S-TL-SSL-TSK	2.03	1.09e-05	(0.0057+2.05e-07)
	A-TL-SSL-TSK	21.97	1.02e-05	(0.0053+1.81e-07)

* The first and the second component inside the bracket are the running time of feature extraction and classification respectively.

2) The average testing time of both algorithms was comparable since they adopted the same the decision function, i.e. Eq. (3.f).

3) The real-time performance can be analyzed by investigating the EEG signal classification process. When raw EEG data were obtained, they were first processed by a feature extraction method (e.g. WPD, STFT or KPCA), and the extracted feature were then processed by a classifier (e.g. S-TL-SSL-TSK or A-TL-SSL-TSK). Thus, the computation time for real-time applications contains two parts, i.e., the running time of the feature extraction method and the running time of the classifier. As shown in Table X, the testing time of A-TL-SSL-TSK and S-TL-SSL-TSK method was comparable, and the difference was due to the variation in running time of different feature extraction methods. The results show that the algorithms (S-TL-SSL-TSK or A-TL-SSL-TSK) developed based on KPCA were much faster than those developed based on WPD or STFT.

It can be concluded from the above analyses that when real-time performance is concerned, if rapid model training is desired, the S-TL-SSL-TSK method is preferable. However, if high recognition accuracy is needed, the A-TL-SSL-TSK is a better choice.

In addition, the running time of S-TL-SSL-TSK and A-TL-SSL-TSK are both acceptable for real-time applications since the main computational cost is feature extraction, as shown in Table X. Furthermore, the KPCA-based S-TL-SSL-TSK or A-TL-SSL-TSK is recommended for applications demanding real-time performance.

VI. CONCLUSIONS

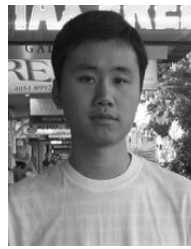
This paper proposes the TL-SSL-TSK model which integrates TL, SSL and TSK fuzzy system model to increase the robustness, accuracy and interpretability of the classifier for EEG signal classification. It also proposes two learning algorithms, S-TL-SSL-TSK and A-TL-SSL-TSK, to train the model. Experimental results show that the proposed approaches can achieve better performance than many state-of-the-art classification algorithms. In addition, according to our experiments, 50 labeled data for source domain and 50 unlabeled data for target domain are usually adequate for the proposed methods to produce satisfactory results, which is also clinically practical. For example, the average accuracy of the two proposed methods are higher than 95% in most cases. Future research will be conducted to reduce the computational

cost of the algorithms, and to extend them to other relevant application domains, including brain-computer interface.

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